Influence of Susceptibility-weighted Imaging on Brain Magnetic Resonance Imaging Diagnostics

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ABSTRACT

Objectives: To evaluate the influence of susceptibility-weighted imaging (SWI) on detection rates and reported results in the diagnosis of various brain conditions, compared with conventional magnetic resonance imaging (MRI).

Methods: Brain MRI was obtained for various indications in 251 patients (115 male, 136 female). The mean age of the patients was 49.91 years. Two neuroradiologists independently evaluated the detection rates and reported results of brain MRI with and without SWI sequences. Statistical analysis was performed by using McNemar's Chi-square test and Cohen's kappa coefficient.

Results: Neuroradiologists 1 and 2 considered SWI to have influenced detection in 51% and 53% of patients, respectively, and to have influenced the reported results in 20% and 18% of patients, respectively. SWI had the strongest influence in the detection rates of vascular disease in 22 patients (100%) and calcification and abscesses in two patients (100%). SWI had the strongest influence on the reported results of vascular disease in 20 patients (91%) and of neurodegenerative / demyelinating in 11 patients (79%). There was excellent inter-observer reliability between neuroradiologists 1 and 2 (kappa value = 0.883-0.936).

Conclusion: SWI is a helpful technique in routine brain MRI sequences, and influences the detection rates and reported results, especially for vascular disease, microbleeds, infection, neurodegenerative / demyelinating disease, and evaluation of intratumoral components. SWI should be added to conventional MRI sequences.

Key Words: Brain; Magnetic resonance imaging

中文摘要

磁敏感加權成像對腦磁共振成像診斷的影響

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目的：與常規磁共振成像（MRI）相比，評估磁敏感加權成像（SWI）對檢測率和各種腦部疾病診斷報告結果的影響。
INTRODUCTION
Susceptibility-weighted imaging (SWI) is a phase-contrast enhancement imaging technique on magnetic resonance imaging (MRI). It offers information about any tissue that has a susceptibility that is different from the surrounding structures, such as deoxygenated blood, hemosiderin, ferritin, and calcium. The local magnetic heterogeneity induced by paramagnetic, diamagnetic, and ferromagnetic substances can result in overall signal loss in gradient recalled echo (GRE) images and a dephase change. The susceptibility effect is highest in GRE techniques at long echo times and high field strengths. The image contrast in magnitude images is acquired by using a high-resolution three-dimensional, fully velocity-compensated, T2*-weighted GRE pulse sequence. Phase images are used to create a phase mask after unwrapping and high pass filtering. This phase mask is then multiplied with the magnitude images to enhance the visibility of small veins and other paramagnetic substances. There are three components to SWI interpretation. First, the original magnitude images highlight susceptibility as signal intensity losses. Second, phase images express the phase differences of tissues. For a left-handed system, veins will look bright on the phase images owing to the paramagnetic effect of deoxygenated blood, and calcium will look dark because of its diamagnetic effect. Third, T2’signal-intensity losses in the magnitude images are used to construct minimum intensity projection (MinIP) images for visualisation of the veins, similar to using maximum intensity projection (MIP) images to visualise arteries in MR angiography.

Several studies have reported that SWI provides additional clinically useful information that is often complementary to conventional MRI sequences in the evaluation of various neurologic disorders, including traumatic brain injury, stroke, intracranial haemorrhage, vascular malformations, neoplasms, and neurodegenerative disorders associated with intracranial calcification or iron deposition.

Since 2009, SWI—including magnitude, phase, and MinIP images—has been included in brain MRI evaluations in Songklanagarind Hospital, Songkhla, Thailand. However, it is time-consuming to scan and perform corrected phase imaging and MinIP imaging. The objectives of this study were to evaluate the influence of SWI on detection rates and reported results of brain MRI, to clarify whether adding SWI to routine imaging protocols is worthwhile.

METHODS
Patient Selection and Data Collection
This retrospective study was conducted at Songklanagarind Hospital. Patients were included who had undergone brain MRI with SWI sequence—including phase, magnitude, and MinIP images—from November 2014 to October 2015. Patients with incomplete SWI information were excluded. Patient demographic data, history of brain surgery and cranial radiation therapy, indication for performing MRI, and imaging manifestations were recorded.

Imaging Acquisition
Two MRI machines with left-handed systems were used; one 1.5-T MRI machine (Ingenia; Philips, the Netherlands), and one 3-T MRI machine (Achieva X-series; Philips). Our routine brain protocol includes axial T1-weighted (T1W) imaging, T2-weighted (T2W) imaging, fluid attenuation inversion recovery (FLAIR) imaging, diffusion-weighted imaging, apparent diffusion coefficient, and GRE imaging; sagittal T1W imaging and
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FLAIR imaging; and coronal T2W imaging. Gadolinium-based contrast administration depends on indications.

For SWI acquisition, the 1.5-T MRI imaging specifications were dStream (Philips), 15-channel head coil, gradient system, maximum gradient strength 45 mT/m, slew rate 200 T/m/s, repetition time 30 ms, echo time 45 ms, fractional anisotropy 15 degrees, pixel size 1.0 × 1.0 mm, slice thickness 1 mm, field of view 180 × 230 mm, acquisition time 258 s, SENSitivity Encoding factor 1.8, and 140 slices. The 3-T MRI imaging specifications were non-multitransmit type using an 8-channel SENSitivity Encoding head coil, Quasar Dual gradient system, maximum gradient strength 80 mT/m, slew rate 200 T/m/s, repetition time 15 ms, echo time 21 ms, fractional anisotropy 10 degrees, pixel size 1.0 × 0.99 mm, slice thickness 0.8 mm, field of view 200 × 240 mm, acquisition time 204 s, SENSitivity Encoding factor 1.3, and 170 slices.

Imaging Analysis
Two experienced neuroradiologists independently interpreted and evaluated all brain MRI images. Radiologist 1 had 30 years of experience and radiologist 2 had 4 years of experience in neurological imaging. The two radiologists assessed whether SWI influenced detection rates for abnormalities, and whether SWI influenced the reported results.

All imaging diagnoses were classified into 10 groups: ischaemic stroke, tumour, vascular disease (vascular malformation and small vessel disease), neurodegenerative / demyelinating disease, infection, calcification, haemorrhage, normal study, inconclusive, and others (air, morning glory syndrome, lymphocytic hypophysitis, syringomyelia, von Hippel–Lindau syndrome, Chiari malformation, extracranial mass, Parry-Romberg syndrome, and colpocephaly).

Statistical Analysis
Data were analysed using EpiData version 3.1. Chi-square test was used to assess the influence of SWI on each diagnostic categorisation. Inter-observer reliability was evaluated using Cohen’s kappa coefficient. A kappa value of 0.01-0.2 indicated slight agreement, 0.21-0.4 indicated fair agreement, 0.41-0.6 indicated moderate agreement, 0.61-0.8 indicated good agreement, and 0.81-0.99 indicated excellent agreement.

RESULTS
Brain MRI with SWI was obtained for various indications in 251 patients (115 male, 136 female, mean age 49.91 years, range 1.25-85 years). Of these, 50 patients received 1.5-T MRI and 201 patients received 3-T MRI.

In all, 114 patients (45.4%) had a history of brain surgery and a few (1.2%) had undergone cranial radiation therapy. The most common indication to perform MRI was postoperative evaluation of brain tumours. Final diagnosis was selected from one of 10 categories (Table 1).

Neuroradiologists 1 and 2 considered that SWI had influenced the detection in 51% and 53% of patients, respectively, and that SWI had influenced the reported results in 20% and 18% of patients (Table 2). The strongest influences of SWI were on the detection rates and diagnosis of vascular disease (Figure 1), calcification (Figure 2), and infection (Figure 3). SWI had the strongest influence on reported results for vascular disease and neurodegenerative / demyelinating disease.

There was excellent agreement between neuroradiologists 1 and 2, with good inter-observer reliability (overall kappa value = 0.883-0.936) for all diagnostic categories.

DISCUSSION
Most previous studies have focused on the ability of SWI to detect magnetic heterogeneity induced by paramagnetic, diamagnetic, and ferromagnetic substances present in various neurological disorders. The present study is concerned with the importance of more detectable findings and how they influence the final diagnosis or reported results.

Table 1. Final diagnosis after 1.5-T or 3-T magnetic resonance imaging.  

<table>
<thead>
<tr>
<th>Final diagnosis</th>
<th>1.5-T MRI (n=50)</th>
<th>3-T MRI (n=201)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Ischaemic stroke</td>
<td>2 (4.0%)</td>
<td>8 (4.0%)</td>
</tr>
<tr>
<td>Tumour</td>
<td>18 (36.0%)</td>
<td>82 (40.8%)</td>
</tr>
<tr>
<td>Vascular disease</td>
<td>5 (10.0%)</td>
<td>17 (8.5%)</td>
</tr>
<tr>
<td>Neurodegenerative / demyelinating disease</td>
<td>2 (4.0%)</td>
<td>12 (6.0%)</td>
</tr>
<tr>
<td>Infection</td>
<td>0</td>
<td>2 (1.0%)</td>
</tr>
<tr>
<td>Calcification</td>
<td>1 (2.0%)</td>
<td>1 (0.5%)</td>
</tr>
<tr>
<td>Haemorrhage</td>
<td>2 (4.0%)</td>
<td>26 (12.9%)</td>
</tr>
<tr>
<td>Normal study</td>
<td>13 (26.0%)</td>
<td>35 (17.4%)</td>
</tr>
<tr>
<td>Inconclusive</td>
<td>0</td>
<td>1 (0.5%)</td>
</tr>
<tr>
<td>Others†</td>
<td>7 (14.0%)</td>
<td>17 (8.5%)</td>
</tr>
</tbody>
</table>

| Data are shown as No. (%) |
| Air, morning glory syndrome, lymphocytic hypophysitis, syringomyelia, von Hippel–Lindau syndrome, Chiari malformation, extracranial mass, Parry-Romberg syndrome, and colpocephaly. |

†
Table 2. Number of patients in which susceptibility-weighted imaging influenced detection rate and/or reported results.*

<table>
<thead>
<tr>
<th>Diagnosis</th>
<th>Influence on detection</th>
<th>Influence on reported results</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>Radiologist 1</td>
<td>Radiologist 2</td>
</tr>
<tr>
<td>Ischaemic stroke (n=10)</td>
<td>3 (30.0%)</td>
<td>3 (30.0%)</td>
</tr>
<tr>
<td>Tumour (n=100)</td>
<td>59 (59.0%)</td>
<td>64 (64.0%)</td>
</tr>
<tr>
<td>Vascular disease (n=22)</td>
<td>22 (100%)</td>
<td>20 (90.9%)</td>
</tr>
<tr>
<td>Neurodegenerative / demyelinating disease (n=14)</td>
<td>11 (78.6%)</td>
<td>11 (78.6%)</td>
</tr>
<tr>
<td>Infection (n=2)</td>
<td>1 (50.0%)</td>
<td>2 (100%)</td>
</tr>
<tr>
<td>Calcification (n=2)</td>
<td>2 (100%)</td>
<td>2 (100%)</td>
</tr>
<tr>
<td>Haemorrhage (n=28)</td>
<td>25 (89.3%)</td>
<td>25 (89.3%)</td>
</tr>
<tr>
<td>Normal study (n=48)</td>
<td>0</td>
<td>0</td>
</tr>
<tr>
<td>Inconclusive (n=1)</td>
<td>0</td>
<td>0</td>
</tr>
<tr>
<td>Others (n=24)†</td>
<td>5 (20.8%)</td>
<td>6 (25.0%)</td>
</tr>
<tr>
<td>Total (n=251)</td>
<td>128 (51.0%)</td>
<td>133 (53.0%)</td>
</tr>
</tbody>
</table>

* Data are shown as No. (%).
† Air, morning glory syndrome, lymphocytic hypophysitis, syringomyelia, von Hippel–Lindau syndrome, Chiari malformation, extracranial mass, Parry-Romberg syndrome, and colpocephaly.

Figure 1. A 58-year-old woman presenting with ataxia. (a) Susceptibility-weighted imaging showing medusa-like hypointensity of developmental venous anomaly at the left cerebellar hemisphere, which was undetectable on gradient recalled echo T2-weighted image. (b) An adjacent cavernous malformation was seen.

Figure 2. An 84-year-old woman presenting with alteration of consciousness. (a) Computed tomography scan showing calcified meningioma at right cerebellar convexity. (b, c) Magnitude and phase images of susceptibility-weighted imaging showing hypointensity corresponding to the areas of denser intratumoural calcification.
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The detection rates and reported results for vascular disease were most strongly influenced by SWI in the present study. In particular, incidental findings of cavernous malformation, developmental venous anomaly, and capillary telangiectasia were influential. Similar to the results of Tsui et al, Barnes et al, and Tong et al, SWI was better in demonstrating low-flow vascular malformations and had an improved detection rate. For high-flow vascular malformations such as arteriovenous malformation and dural arteriovenous fistula, both MinIP and MIP techniques can improve the image quality. In the present study, SWI also demonstrated improvements in detection rates and diagnosis for abnormal venous structures in two patients with arteriovenous malformations that were in agreement with previous studies. Our study is in agreement with a previous study that reported that SWI is a useful method to evaluate venous sinus thrombosis by demonstrating an increased deoxyhaemoglobin concentration in the area of venous stasis and collateral slow flows.

Calcification cannot be differentiated from haemorrhage by a GRE image. Both cause local magnetic field changes and appear as hypointensity. The phase image of SWI can distinguish these lesions; calcification is diamagnetic, whereas haemorrhage is paramagnetic, resulting in opposite signal intensities. The detection rate of SWI for intracranial calcification has previously been reported as 98.2%, which was significantly higher than T1W and T2W images. This was not significantly different from the detection rate for calcification in the present study (100%, n=2) [Table 2].

The present study also agreed with another study that reported SWI is more sensitive than T1W and T2W images in identifying chronic haemorrhagic lesions and cerebral microbleeds. However, few of our patients were affected by these diagnostic results.

A recent study reported that the dual rim sign is the most specific imaging feature differentiating pyogenic brain abscess from necrotic glioblastoma on SWI. The outer hypointense rim corresponds to the enhanced abscess capsule, with production of paramagnetic free radicals caused by macrophages. The inner hyperintense rim is granulation tissue between the abscess cavity and

Figure 3. A 36-year-old woman presenting with fever and headache. (a) Axial T2-weighted image and (b) gradient recalled echo T2-weighted image showing a smooth thin hypointense rim. (c) Susceptibility-weighted imaging showing dual rim sign, defined as outer rim hypointensity and inner rim hyperintensity, a specific feature of pyogenic abscess. (d) Diffusion-weighted image and (e) apparent diffusion coefficient image showing restricted water diffusion. (f) Gadolinium-enhanced T1-weighted image showing smooth thin rim enhancement. Stereotactic biopsy found frank pus.
fibrocollagenous capsule. This dual rim sign was seen in two patients in the present study who were finally diagnosed as having pyogenic abscess.

Abnormally elevated iron levels are evident in many neurodegenerative disorders, including Parkinson’s disease, Alzheimer’s disease, Huntington’s disease, and amyotrophic lateral sclerosis. However, iron deposition is commonly seen with increasing age.\textsuperscript{13,14} It is more difficult to differentiate normal and pathologic mineralisation with advanced age because physiologic deposition such as calcium and iron are more pronounced in older patients. Comparison with age-matched SWI images can be helpful. SWI filtered phase imaging is suitable for demonstration of increased iron content and shows a better distinction between the pars compacta and the pars reticulata of the substantia nigra, which contains iron. In idiopathic Parkinson’s disease, there is evidence of increased iron in the substantia nigra. SWI is a potentially useful imaging tool to identify iron deposition as a biomarker for disease progression. Accurate localisation of the subthalamic nucleus can be achieved on SWI, allowing safe direct targeting for placement of electrodes in the treatment of Parkinson’s disease.\textsuperscript{15} In patients with multiple sclerosis, very high iron deposition is seen in deep grey matter structures such as the pulvinar, caudate nucleus, putamen, and thalamus. Iron is also seen in the ring-like structures around some multiple sclerosis lesions that are often visible on SWI but not in conventional images.\textsuperscript{13,14,16} In 8 of 12 patients with Parkinson’s disease and one patient with multiple sclerosis, phase images were potentially helpful to detect and diagnose the diseases, but iron deposition was poorly seen or not visible on conventional MRI. Therefore, SWI should be performed in cases of neurodegenerative and demyelinating diseases, especially Parkinson’s disease and multiple sclerosis. However, clinical correlation is important for diagnosis, because iron deposition is also part of the normal ageing process.

SWI can demonstrate internal characteristics of brain tumours including haemorrhage, neovascularity, calcification, and cystic component. It improves detection rates of tumour-related haemorrhage compared with GRE.\textsuperscript{17,18} High-graded tumours such as glioblastoma often have a haemorrhagic component, which may be useful for staging. Kim et al.\textsuperscript{19} assessed the added value provided by SWI in the differential diagnosis of solitary enhancing brain lesions compared with conventional MRI alone. Preoperative SWI evaluation of a butterfly mass in the present study revealed multiple haemorrhagic foci on SWI; therefore, they were differentiated from lymphoma and ultimately diagnosed as glioblastoma. However, most patients in the present study came for interval follow-up after treatment for brain tumours, including surgery and radiation therapy. Post-treatment SWI detected haemorrhage and microbleeds more often than did conventional MRI; however, this did not influence the reported results.

Several studies have reported that SWI is more sensitive in detecting haemorrhage within an infarct than CT and T2*-weighted imaging or GRE scans.\textsuperscript{20-22} Furthermore, SWI can detect haemorrhagic transformation earlier than CT.\textsuperscript{13,17,20,21,23} SWI is also helpful for monitoring complications after revascularisation therapy. Decreased arterial blood oxygenation causes increased deoxyhaemoglobin in the infarcted area; the increased hypointensity along the affected cortex is detected on T2*-weighted imaging, and both magnitude and phase images of SWI.\textsuperscript{24} The difference between arterial and venous vessels cannot be seen with conventional MRI sequences. Prominent veins within areas of impaired perfusion allow the identification of penumbral brain tissue. In 3 of 10 patients with stroke in the present study, haemorrhage and microbleeds were more distinctive in the infarcted area on SWI than on conventional MRI. In one of these patients, SWI revealed transmedullary veins that were not seen on conventional MRI.

Our study had a few limitations. First, despite the large number of patients, they were not proportionately distributed in each group. Second, the final diagnosis was made by various methods, including pathological results in cases of surgery, comparison with previous studies or interval follow-up, and by consensus of the two neuroradiologists.

**CONCLUSION**

SWI is a helpful technique on routine brain MRI that has an influence on detection rates and reported results, especially for vascular diseases, microbleeds, infection, neurodegenerative / demyelinating disease, and evaluation of intratumoural components. It is recommended that SWI should be added to conventional MRI sequences.

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